

# Bioimaging of Hyaluronate–Interferon $\alpha$ Conjugates Using a Non-Interfering Zwitterionic Fluorophore

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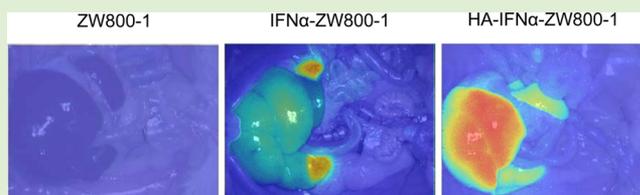
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## Supporting Information

**ABSTRACT:** We conducted real-time bioimaging of the hyaluronate–interferon  $\alpha$  (HA–IFN $\alpha$ ) conjugate using a biologically inert zwitterionic fluorophore of ZW800-1 for the treatment of hepatitis C virus (HCV) infection. ZW800-1 was labeled on the IFN $\alpha$  molecule of the HA–IFN $\alpha$  conjugate to investigate its biodistribution and clearance without altering its physicochemical and targeting characteristics. Confocal microscopy clearly visualized the effective *in vitro* cellular uptake of the HA–IFN $\alpha$  conjugate to HepG2 cells. After verifying the biological activity in Daudi cells, we conducted the pharmacokinetic analysis of the HA–IFN $\alpha$  conjugate, which confirmed its target-specific delivery to the liver with a prolonged residence time longer than that of PEGylated IFN $\alpha$ . *In vivo* and *ex vivo* bioimaging of the ZW800-1-labeled HA–IFN $\alpha$  conjugate directly showed real-time biodistribution and clearance of the conjugate that are consistent with the biological behaviors analyzed by an enzyme-linked immunosorbent assay. Furthermore, the elevated level of OAS1 mRNA in the liver confirmed *in vivo* antiviral activity of HA–IFN $\alpha$  conjugates. With the data taken together, we could confirm the feasibility of ZW800-1 as a biologically inert fluorophore and target-specific HA–IFN $\alpha$  conjugate for the treatment of HCV infection.



## INTRODUCTION

Hepatitis C virus (HCV) is the main cause of chronic liver diseases,<sup>1</sup> infecting ~200 million people worldwide.<sup>2</sup> In addition, more than 350000 people die from liver diseases caused by HCV infection every year.<sup>3</sup> There have been numerous clinical trials<sup>4,5</sup> for the treatment of HCV infection, but the only outcome from the past is the clinical use of interferon  $\alpha$  (IFN $\alpha$ ) derivatives.<sup>1,6</sup> Currently, there are several kinds of polymer–IFN $\alpha$  conjugate formulations available for treating liver diseases. Among them, PEGylated interferon  $\alpha$  (PEG–IFN $\alpha$ ) has been successfully commercialized under the trade names PEGASYS and PEG-Intron.<sup>7–9</sup> However, PEGylation was intended to bypass liver for long-term circulation of biopharmaceuticals, which might not be a good strategy for the treatment of liver diseases. PEG–IFN $\alpha$  resulted in an unexpectedly low sustained virologic response of 39% in clinical tests.<sup>10</sup> Despite the recent announcement on two approved drugs and dozens more in the pipeline,<sup>6</sup> IFN $\alpha$  therapy remains an important remedy for the treatment of HCV infection.

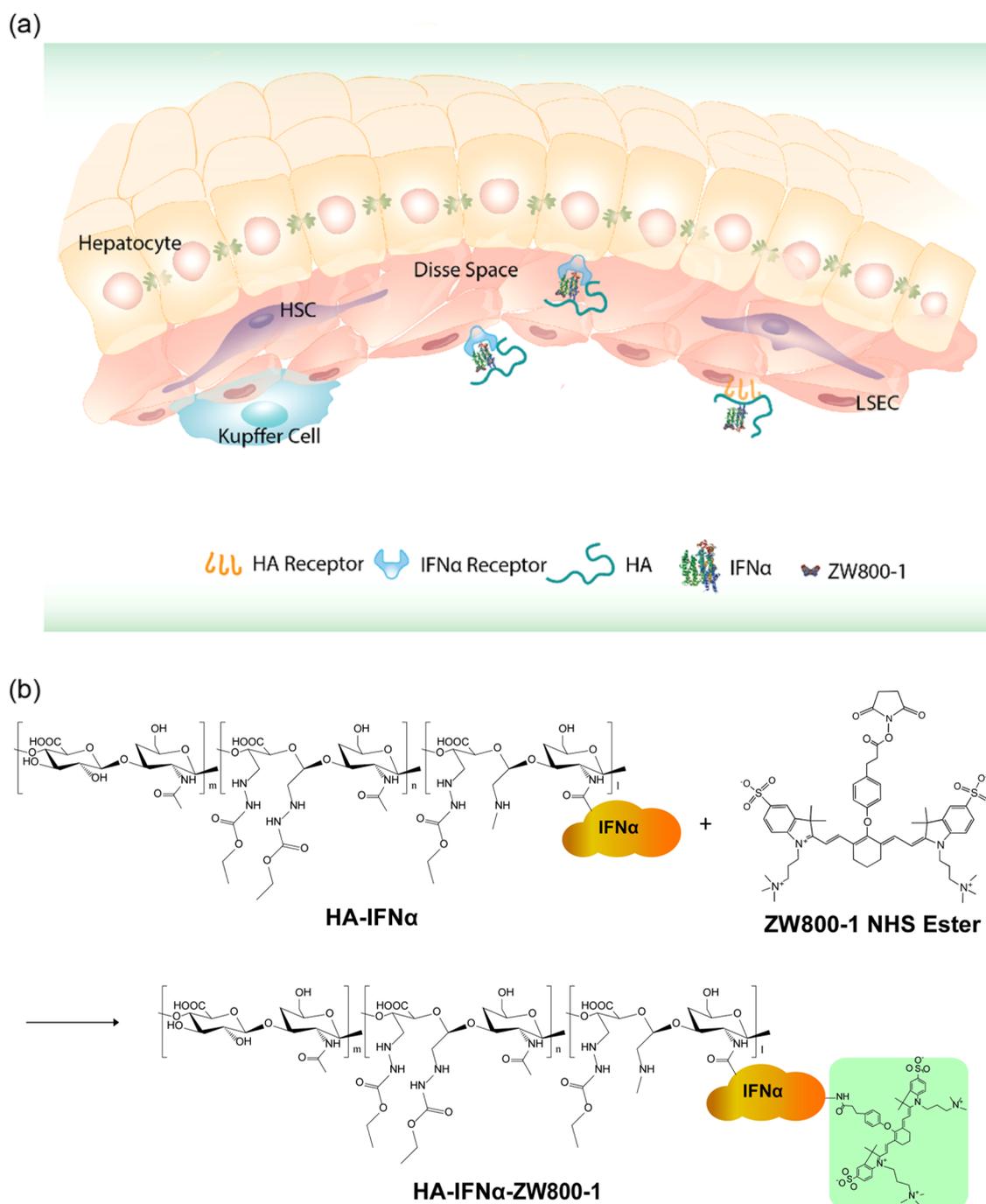
Hyaluronate (HA), a biocompatible, biodegradable, and non-toxic polysaccharide, has been extensively investigated as a

target-specific drug delivery carrier.<sup>11,12</sup> In our previous work, we successfully investigated the bioconjugation efficiency and *in vitro* and *in vivo* biological activity of the HA–IFN $\alpha$  conjugate for the treatment of HCV infection.<sup>10</sup> However, *in vivo* dynamics and clearance were not explored in detail without adequate imaging agents. The use of hydrophobic metal-containing quantum dots (QDots) as an imaging probe might result in alteration of the biological behaviors of the conjugates.<sup>13–16</sup> In addition, unconjugated or detached QDots might contaminate the target-specific HA in the body during excretion and metabolic processes, causing various side effects because of their inherent toxicity.<sup>17,18</sup> To circumvent these issues, a zwitterionic (ZW) fluorophore of ZW800-1 has been developed to investigate the *in vivo* mechanism, disease targeting, and biodistribution of biomolecules.<sup>19,20</sup> In addition, it can be easily conjugated to other biomolecules such as targeting moieties in the forms of an aptamer, a peptide, and a protein.

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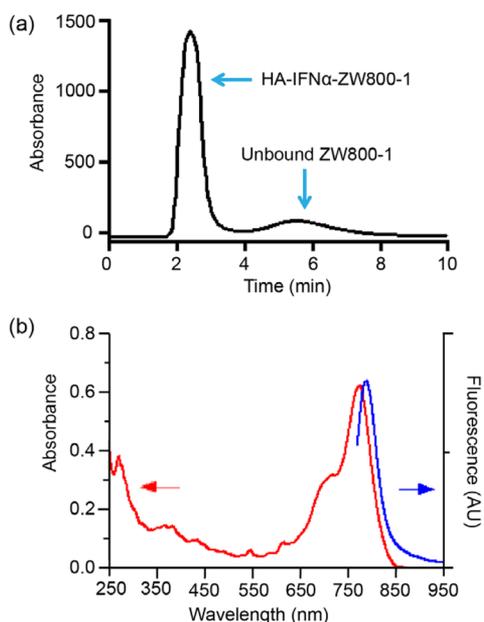
**Figure 1.** Schematic illustration of (a) the targeted delivery of HA-IFN $\alpha$  conjugates to the liver and (b) the labeling of the HA-IFN $\alpha$  conjugate with zwitterionic dye ZW800-1.

In this study, we conjugated a ZW-NIR fluorophore of ZW800-1 to the amine group of IFN $\alpha$  in HA-IFN $\alpha$  conjugates. Because ZW800-1 has a net charge of zero and an emission wavelength of 800 nm in the near-infrared (NIR) window, we could avoid potentially nonspecific tissue uptake and serum protein association,<sup>19,20</sup> allowing *in vivo* visualization for the long-term biodistribution and clearance of HA-IFN $\alpha$  conjugates without the first-pass effect of lipophilic bioconjugates.<sup>21,22</sup> After *in vitro*, *in vivo*, and *ex vivo* bioimaging of the ZW800-1-labeled HA-IFN $\alpha$  conjugate, we assessed the antiviral activity of HA-IFN $\alpha$  conjugates and discussed the feasibility of ZW800-1 as a biologically inert fluorophore for

further bioimaging applications and target-specific HA-IFN $\alpha$  conjugates for the treatment of HCV infection.

## EXPERIMENTAL SECTION

**Synthesis of the HA-IFN $\alpha$ -ZW800-1 Conjugate.** The HA-IFN $\alpha$  conjugate was synthesized as we previously reported.<sup>30</sup> PEG-IFN $\alpha$  (PEG-Intron, Merck) was used as a positive control. To synthesize ZW800-1 NHS ester, 2 equiv of dipyrrolidino(*N*-succinimidyl)oxycarbonyl hexafluorophosphate in dimethyl sulfoxide was mixed with 5 equiv of diisopropylethylamine at room temperature in the dark.<sup>19,20</sup> After being stirred for 3 h, the reaction mixture was precipitated with an excess of ethyl acetate. The precipitate was washed with a 1:1 mixture of ethyl acetate and acetone thrice and



**Figure 2.** Characterization of the HA-IFN $\alpha$ -ZW800-1 conjugate by (a) gel filtration chromatography and (b) spectrophotometry.

dried in vacuum. The purity was confirmed to be higher than 98% by reversed-phase high-performance liquid chromatography (770 nm absorbance) and matrix-assisted laser desorption/ionization time of flight. The primary amine on IFN $\alpha$  in the HA-IFN $\alpha$  conjugate was conjugated with the ZW800-1 NHS ester at a 1:2 (IFN $\alpha$ :dye) ratio in

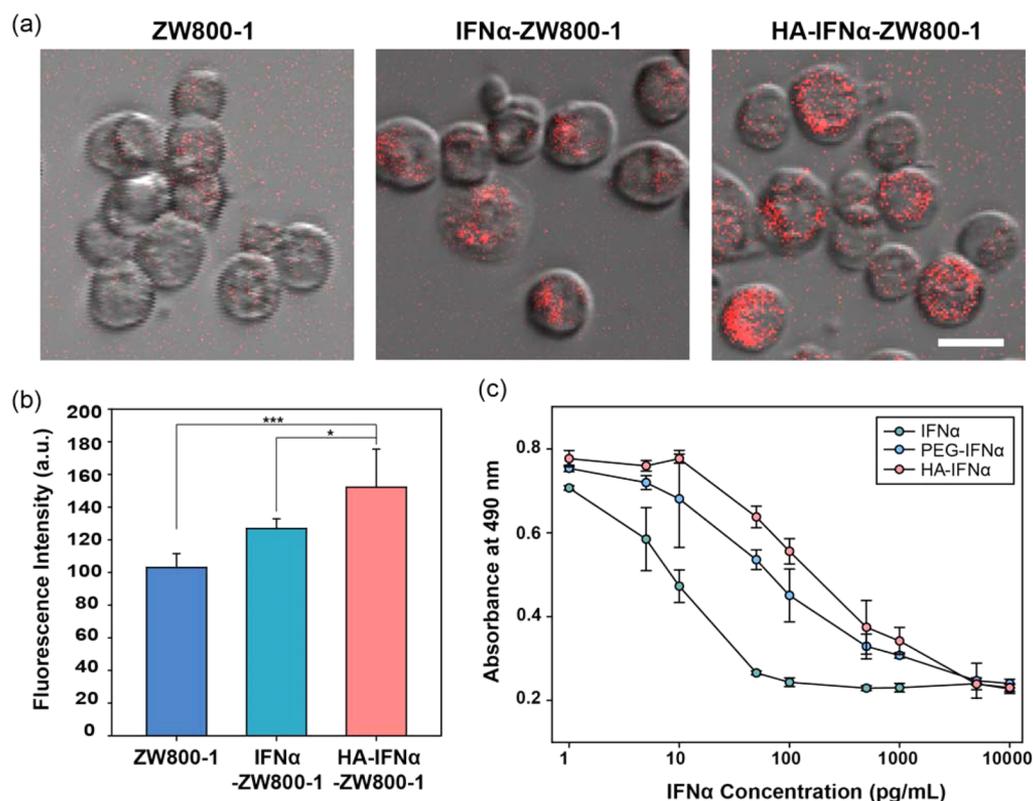
PBS (pH 7.8), followed by purification using gel filtration chromatography (GFC). For comparison, the IFN $\alpha$ -ZW800-1 conjugate was also prepared by the conjugation of free IFN $\alpha$  with the same amount of ZW800-1 NHS ester.

#### **In Vitro Bioimaging of the HA-IFN $\alpha$ -ZW800-1 Conjugate.**

Human hepatocarcinoma cells (HepG2, ATCC, Manassas, VA) were cultured at 37 °C and 5% CO<sub>2</sub> in DMEM containing 10% fetal bovine serum (FBS) and 10 IU/mL antibiotics (penicillin). HepG2 cells ( $5 \times 10^4$ ) were seeded and incubated in a six-well culture dish for 24 h, followed by the replacement of medium with DMEM containing 1% FBS. One milliliter of ZW800-1, IFN $\alpha$ -ZW800-1 conjugate, or HA-IFN $\alpha$ -ZW800-1 conjugate was added to each well at a concentration of 2  $\mu$ M and incubated for 2 h.<sup>15</sup> Cells were washed with PBS, fixed with 4% paraformaldehyde in PBS, washed again with PBS twice, and observed with a fluorescence microscope at a magnification of 200 $\times$ . The internalized HA-IFN $\alpha$ -ZW800-1 conjugate in the cytoplasm was excited at 700 nm and visualized through a long pass emission filter (Chroma Technology Co., Brattleboro, VT).

#### **In Vitro Biological Activity of the HA-IFN $\alpha$ Conjugate.**

Human Daudi cells (Korean Cell Line Bank, Seoul, Korea) were cultured in RPMI 1640 (Mediatech, Herndon, VA) supplemented with 10% FBS and 1% antibiotics in a humidified incubator at 37 °C under 5% CO<sub>2</sub> in air. Cells were seeded onto sterilized 18 mm diameter glass coverslips in 96-well plates ( $2 \times 10^4$  cells per well). A serial dilution of protein samples was prepared in assay medium, and 50  $\mu$ L of the diluted protein samples was added to the test wells in triplicate. The plates were incubated at 37 °C in a humidified 5% CO<sub>2</sub> tissue culture incubator for 4 days. Then, 20  $\mu$ L of Cell Titer 96 Aqueous One Solution Reagent (Promega, Madison, WI) was added to each well, which was incubated additionally at 37 °C for 2 h. The absorbance was measured at 490 nm using a microplate reader (EMax, Molecular Devices).



**Figure 3.** (a) Confocal microscopic imaging of the intracellular uptake of ZW800-1, IFN $\alpha$ -ZW800-1, and HA-IFN $\alpha$ -ZW800-1 conjugates into HepG2 cells. (b) Quantitative fluorescence analysis of the samples taken up by HepG2 cells. Statistical analysis was conducted for the HA-IFN $\alpha$ -ZW800-1 conjugate vs other groups (\* $P < 0.05$ , and \*\*\* $P < 0.001$ ). (c) Antiproliferation effect of IFN $\alpha$ , PEG-IFN $\alpha$ , and HA-IFN $\alpha$  conjugates in Daudi cells.

**In Vivo and ex Vivo Bioimaging of the HA-IFN $\alpha$ -ZW800-1 Conjugate.** Animals were housed in an AAALAC-certified facility. All animal studies were performed under the supervision of BIDMC IACUC in accordance with approved institutional protocol 058-2014. For intraoperative hepatic imaging, male Sprague-Dawley (SD) rats weighing 250–300 g were purchased from Charles River Laboratories (Wilmington, MA). Prior to surgery, animals were anesthetized with 100 mg/kg of ketamine and 10 mg/kg of xylazine intraperitoneally (Webster Veterinary, Fort Devens, MA). After intravenous injection of ZW800-1, the IFN $\alpha$ -ZW800-1 conjugate, or the HA-IFN $\alpha$ -ZW800-1 conjugate (50 nmol) at the same concentration of ZW800-1 into SD rats, intraoperative imaging was performed at each designated time point up to 24 h to observe the initial biodistribution and clearance. For long-term imaging, SD rats were sacrificed 1, 2, 4, 7, and 10 days after injection of HA-IFN $\alpha$ -ZW800-1 conjugates (50 nmol), and their organs were dissected for quantitative fluorescence imaging. *In vivo* and *ex vivo* images were obtained by merging the optical image and the corresponding fluorescence image.

**Intraoperative Image Analysis.** As we previously described in detail,<sup>19</sup> bioimaging was conducted using a FLARE imaging system. At predetermined time points, the fluorescence (FL) and background (BG) intensities of a region of interest (ROI) over each organ and/or tissue were quantified using custom FLARE software. The signal-to-background ratio (SBR) was calculated using ImageJ version 1.45q. All NIR fluorescence images were normalized identically for all conditions. At least three to five animals were analyzed at each time point.

**Biodistribution of the HA-IFN $\alpha$  Conjugate by an Enzyme-Linked Immunosorbent Assay (ELISA).** After intravenous injection of PEG-IFN $\alpha$  and HA-IFN $\alpha$  conjugates containing 70  $\mu$ g of IFN $\alpha$  into SD rats (250 g), animals were sacrificed 1, 3, 7, and 14 days postinjection. The blood serum was collected by centrifugation at 3500 rpm for 30 min, and the same weight of liver tissue was homogenized for 10 min, followed by sonication for 1 min. The IFN $\alpha$  content in the blood and liver tissue was quantified with IFN $\alpha$  ELISA kits (PBL InterferonSource, Piscataway, NJ).

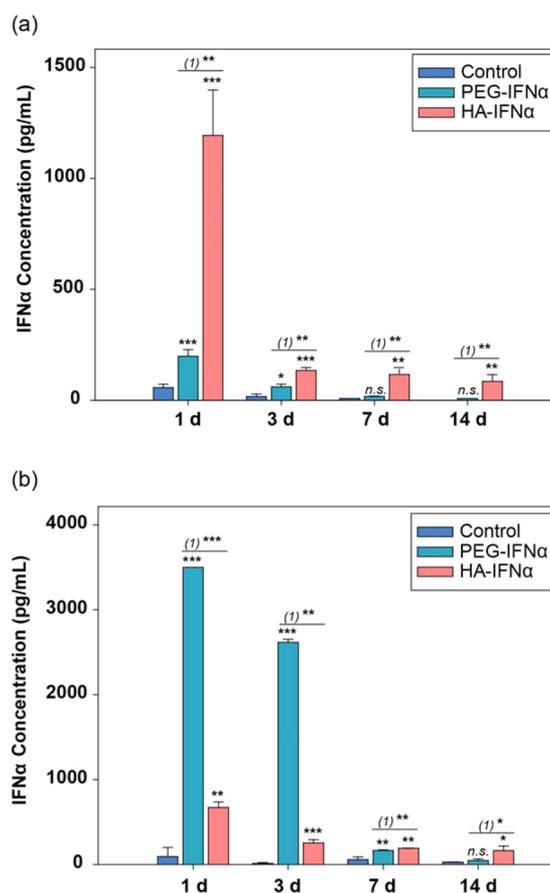
**In Vivo Antiviral Effect of HA-IFN $\alpha$  Conjugates.** After subcutaneous injection of PEG-IFN $\alpha$  and HA-IFN $\alpha$  conjugates containing 70  $\mu$ g of IFN $\alpha$  into SD rats (250 g), animals were sacrificed 2 and 4 days postinjection. The same weight of liver tissues was collected for the analysis of IFN $\alpha$  content by an ELISA and OAS1-expressing mRNA (OAS1 mRNA) level by reverse transcriptase polymerase chain reaction (RT-PCR) (Alpha Unit Block Assembly for PTC DNA Engine Systems, MJ Research).

**Statistical Analysis.** Statistical analysis was conducted via the two-way analysis of variance (ANOVA) test using SigmaPlot 10.0 (Systat Software Inc., San Jose, CA). A *P* value of <0.05 was considered statistically significant. Data are expressed as means  $\pm$  the standard deviation from several separate experiments (*n* = 3).

## RESULTS AND DISCUSSION

**Synthesis of the HA-IFN $\alpha$ -ZW800-1 Conjugate.** Figure 1a shows the schematic illustration for dual targeted delivery of HA-IFN $\alpha$  conjugates for the treatment of HCV infection. The HA-IFN $\alpha$  conjugates can interact with both the receptor and the HA receptor on liver sinusoidal endothelial cells (LSEC), penetrating into the perisinusoidal space (space of Disse) through LESC fenestration.<sup>15,23,24</sup> Accordingly, HA-IFN $\alpha$  conjugates can be efficiently delivered to and accumulate in the liver. As a proof of concept, we synthesized and compared HA-IFN $\alpha$  conjugates (MW of HA = 17 kDa) with PEG-Intron (PEG-IFN $\alpha$ ), a commercially available PEGylated IFN $\alpha$  (MW of PEG = 12 kDa). The lysine residue of IFN $\alpha$  was directly conjugated with ZW800-1 NHS ester by the conventional NHS ester reaction (Figure 1b). The resulting HA-IFN $\alpha$ -ZW800-1 conjugate was purified by GFC to remove unconjugated fluorophores.

As shown in Figure 2, the GFC trace shows the successful conjugation with two isolated peaks indicating the HA-IFN $\alpha$ -

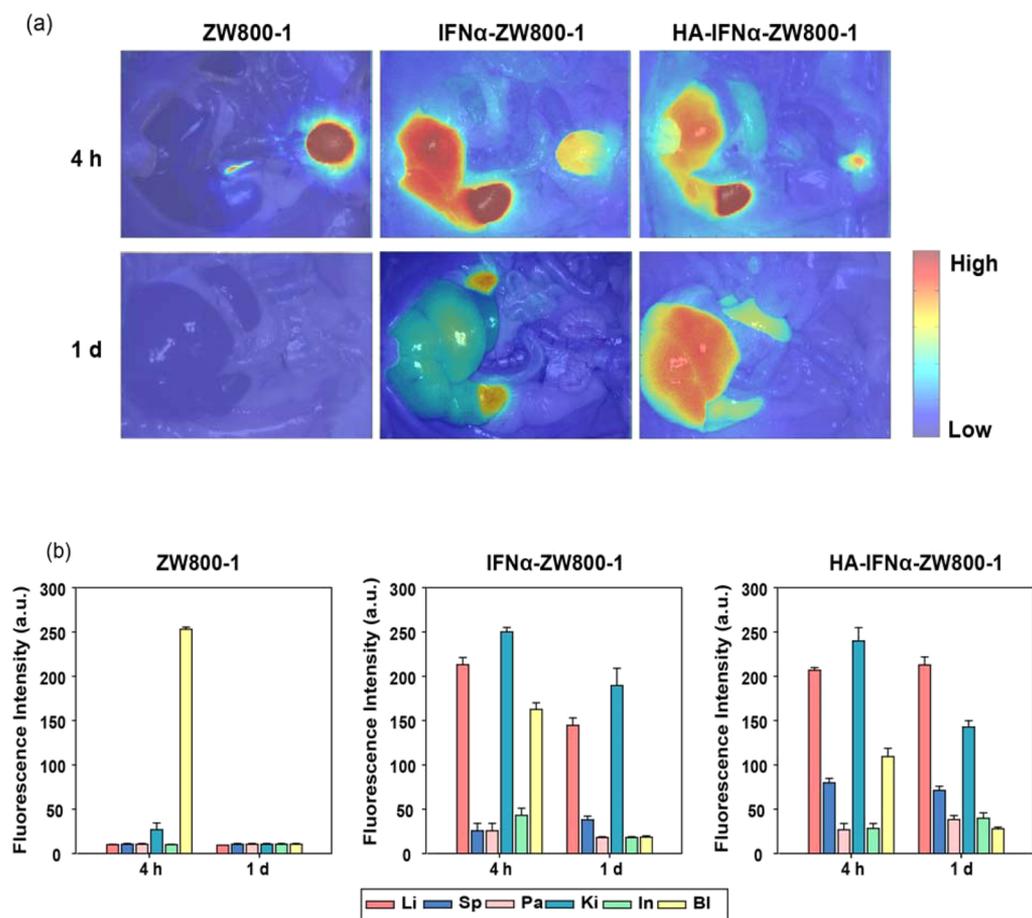


**Figure 4.** Pharmacokinetic analysis of PEG-IFN $\alpha$  and HA-IFN $\alpha$  conjugates by an ELISA in (a) the liver and (b) blood serum after intravenous injection. PBS was used as a negative control. Statistical analysis was conducted for the control vs PEG-IFN $\alpha$  and HA-IFN $\alpha$  conjugates (\**P* < 0.05; \*\**P* < 0.01; \*\*\**P* < 0.001). (1) represents the PEG-IFN $\alpha$  vs HA-IFN $\alpha$  conjugate.

ZW800-1 conjugate (2.5 min) and unreacted ZW800-1 (5.5 min). The purified HA-IFN $\alpha$ -ZW800-1 conjugate was characterized with a spectrophotometer ( $\lambda_{\max \text{ Abs}} = 775 \text{ nm}$ ;  $\lambda_{\max \text{ FL}} = 788 \text{ nm}$ ). The conjugation efficiency was estimated from the ratio of extinction coefficients of ZW800-1 ( $\epsilon_{772} = 249000 \text{ M}^{-1} \text{ cm}^{-1}$ ) and IFN $\alpha$  ( $\epsilon_{280} = 18000 \text{ M}^{-1} \text{ cm}^{-1}$ ) with correction for 5% measured absorbance at 280 nm due to ZW800-1. The calculated labeling ratios for the HA-IFN $\alpha$ -ZW800-1 and IFN $\alpha$ -ZW800-1 conjugates were 0.215 and 0.273, respectively, which were determined by using the formula  $(\text{Abs}_{772}/\epsilon_{772})/[(\text{Abs}_{280} - 0.05 \times \text{Abs}_{772})/\epsilon_{280}]$ . We purposely conjugated small numbers of dyes on the protein to prevent the disruption of activity by the conjugated fluorophores. With the minimal conjugation of ZW800-1, it was possible to visualize the HA-IFN $\alpha$  conjugate because of its high quantum yield (QY = 15%) and high extinction coefficient ( $\epsilon = 249000 \text{ M}^{-1} \text{ cm}^{-1}$ ), as we reported elsewhere.<sup>19,20</sup>

### In Vitro Biological Activity of the HA-IFN $\alpha$ Conjugate.

Figure 3a shows fluorescence microscopic images for *in vitro* cellular uptake of ZW800-1, IFN $\alpha$ -ZW800-1, and HA-IFN $\alpha$ -ZW800-1 conjugates into human hepatocarcinoma HepG2 cells. The rate of intracellular uptake of HA-IFN $\alpha$ -ZW800-1 conjugates was significantly higher than that of IFN $\alpha$ -ZW800-1 (\**P* < 0.05) or ZW800-1 alone (\*\*\**P* < 0.001) as shown in Figure 3b. Because hepatocellular carcinoma HepG2 cells have both IFN $\alpha$  and HA receptors,<sup>15,25,26</sup> the HA-IFN $\alpha$  conjugate



**Figure 5.** (a) *In vivo* biodistribution of ZW800-1, IFN $\alpha$ -ZW800-1, and HA-IFN $\alpha$ -ZW800-1 conjugate in SD rats 4 and 24 h after intravenous injection. (b) Quantitative fluorescence analysis of intraoperative major organs. Abbreviations: Li, liver; Sp, spleen; Pa, pancreas; Ki, kidney; In, intestine; Bl, bladder.

can easily bind to the cells by the dual targeting effect of HA and IFN $\alpha$ . In addition, zwitterionic ZW800-1 has no affinity for the cellular membrane<sup>19,20</sup> without interfering with the *in vitro* cellular uptake of the HA-IFN $\alpha$ -ZW800-1 conjugate via HA receptor-mediated endocytosis.<sup>11–13</sup>

Figure 3c shows the *in vitro* biological activity of the HA-IFN $\alpha$  conjugate, which was confirmed by an antiproliferation assay using human B-lymphoblasts of Daudi cells. Daudi cells are known to be arrested in the G<sub>0</sub>/G<sub>1</sub> phase of the cell cycle in the presence of IFN $\alpha$ .<sup>10,27</sup> The antiproliferation activity of the HA-IFN $\alpha$  conjugate was compared with those of PEG-IFN $\alpha$  and IFN $\alpha$  by measuring the concentration for 50% inhibition of cell growth (IC<sub>50</sub>). The antiproliferation effect of the HA-IFN $\alpha$  (IC<sub>50</sub> = 165.8 pg/mL) conjugate was significantly lower than that of native IFN $\alpha$  (IC<sub>50</sub> = 6.6 pg/mL; \*\**P* < 0.01) but comparable to that of PEG-IFN $\alpha$  (IC<sub>50</sub> = 70.0 pg/mL; *P* > 0.05). Because HA is biodegradable in the body, the biological activity of the HA-IFN $\alpha$  conjugate might increase after degradation by hyaluronidase in the body.

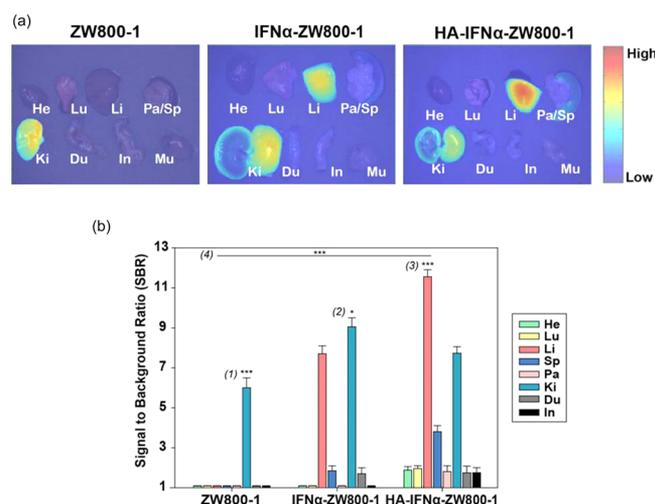
**Pharmacokinetics of the HA-IFN $\alpha$  Conjugate.** Because the residence time of IFN $\alpha$  in blood is significantly important for therapeutic efficacy,<sup>28,29</sup> we analyzed the amount of PEG-IFN $\alpha$  and HA-IFN $\alpha$  conjugates in the blood serum and the liver (Figure 4). After the injection of PEG-IFN $\alpha$  and HA-IFN $\alpha$  conjugates containing 70  $\mu$ g of IFN $\alpha$  intravenously into SD rats, blood serum was collected at predetermined time points, and the liver was dissected and homogenized to

measure the IFN $\alpha$  content by an ELISA. While PEG-IFN $\alpha$  was predominantly detected in the bloodstream on day 1 (\*\**P* < 0.001) and day 3 (\*\**P* < 0.01), HA-IFN $\alpha$  conjugates mainly accumulated in the liver on days 1 and 3 (\*\**P* < 0.01), remaining for up to 14 days postinjection. The results clearly indicate that the HA-IFN $\alpha$  conjugate can be target-specifically delivered to the liver in comparison to PEG-IFN $\alpha$ . Remarkably, the HA-IFN $\alpha$  conjugate remained longer in the liver than PEG-IFN $\alpha$  with a significant difference on days 7 and 14. The presence of PEG-IFN $\alpha$  was minimal and similar to that of the negative control in 7 days (*P* > 0.05). As well-known, PEGylation is intended to increase the blood circulation of conjugated therapeutics bypassing the liver. However, nonspecifically delivered PEG-IFN $\alpha$  was reported to cause serious side effects after repeated injections.<sup>30</sup> On the contrary, there are abundant HA receptors in the liver, including CD44 and HARE, which can promote the active uptake of HA-IFN $\alpha$  conjugates to the liver synergistically and concurrently with the existing IFN $\alpha$  receptors.<sup>11</sup> Armed with these results, we further investigated the long-term biodistribution and clearance of HA-IFN $\alpha$ -ZW800-1 conjugates *in vivo*.

**Real-Time Biodistribution of the HA-IFN $\alpha$ -ZW800-1 Conjugate.** As shown in Figure 5, NIR fluorescence imaging with the FLARE system visualized the real-time intraoperative biodistribution of HA-IFN $\alpha$ -ZW800-1 conjugates after injection of 50 nmol of the conjugate via the penile vein into SD rats (Supporting Video 1). As controls, ZW800-1 and the

IFN $\alpha$ -ZW800-1 conjugate were also tested for comparison.<sup>17,18</sup> ZW800-1 was distributed into the whole body in 30 min and cleared out within 4 h through kidneys to bladder without nonspecific uptake in major organs.<sup>19,20</sup> Almost no fluorescence signal remained in the liver, and >75% of the injected dose was found in the bladder. On the other hand, both IFN $\alpha$ -ZW800-1 and HA-IFN $\alpha$ -ZW800-1 conjugates saturated kidneys first and then gradually accumulated in the liver between 30 and 240 min. The intensity of IFN $\alpha$ -ZW800-1 signals was maximal in the liver at 4 h, whereas the HA-IFN $\alpha$ -ZW800-1 conjugate steadily accumulated in the liver for up to 24 h.

Figure 6 shows the anatomic analysis of dissected organs 24 h post-intravenous injection of ZW800-1, IFN $\alpha$ -ZW800-1,

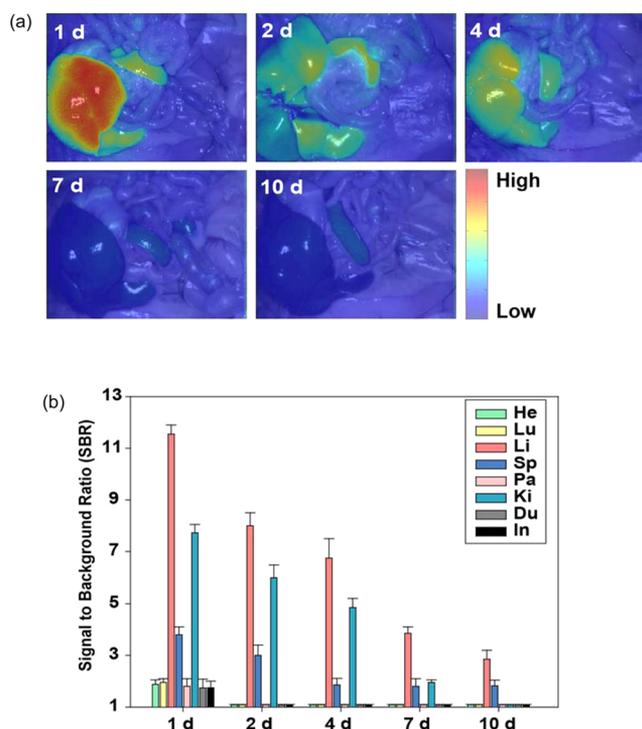


**Figure 6.** (a) *Ex vivo* biodistribution of ZW800-1, IFN $\alpha$ -ZW800-1, and HA-IFN $\alpha$ -ZW800-1 conjugate in SD rats 24 h after intravenous injection. (b) Quantitative fluorescence analysis of dissected organs 24 h postinjection for the biodistribution. Abbreviations: He, heart; Lu, lung; Li, liver; Sp, spleen; Pa, pancreas; Ki, kidney; Du, duodenum; In, intestine. Statistical analysis was conducted for (1) kidney vs other organs treated with ZW800-1 (\*\*\*)  $P < 0.001$ , (2) kidney vs liver treated with IFN $\alpha$ -ZW800-1 (\* $P < 0.05$ ), (3) liver vs other organs treated with the HA-IFN $\alpha$ -ZW800-1 conjugate (\*\*\*)  $P < 0.001$ , and (4) liver treated with the HA-IFN $\alpha$ -ZW800-1 conjugate vs IFN $\alpha$ -ZW800-1 and ZW800-1 (\*\*\*)  $P < 0.001$ .

and HA-IFN $\alpha$ -ZW800-1 conjugate. The level of targeted delivery of the HA-IFN $\alpha$ -ZW800-1 conjugate to the liver was significantly higher than those of two controls (\*\*\*)  $P < 0.001$ . Although the biodistribution trend of IFN $\alpha$ -ZW800-1 was similar to that of the HA-IFN $\alpha$ -ZW800-1 conjugate, the longitudinal uptake was different in the liver and kidney. In accordance with the results in Figure 5, IFN $\alpha$ -ZW800-1 was rapidly degraded and accumulated in the kidney, showing the highest level in 24 h. However, the HA-IFN $\alpha$ -ZW800-1 conjugate gradually decreased in the kidney and increased in the liver with increasing time. Because HA receptors of CD44 and LYVE-1 are highly expressed on renal parenchymal cells<sup>31</sup> and in the renal lymphatic vessel,<sup>32</sup> HA-IFN $\alpha$ -ZW800-1 conjugates showed a high rate of uptake in the kidney. In addition, a high rate of uptake of the HA-IFN $\alpha$ -ZW800-1 conjugate in the spleen also resulted from the high level of expression of HA receptors on lymphatics.<sup>32</sup> The SBR of the HA-IFN $\alpha$ -ZW800-1 conjugate in the liver was remarkably higher for up to 24 h postinjection. The results clearly indicate

that HA-IFN $\alpha$ -ZW800-1 conjugates can be target-specifically delivered to the liver.

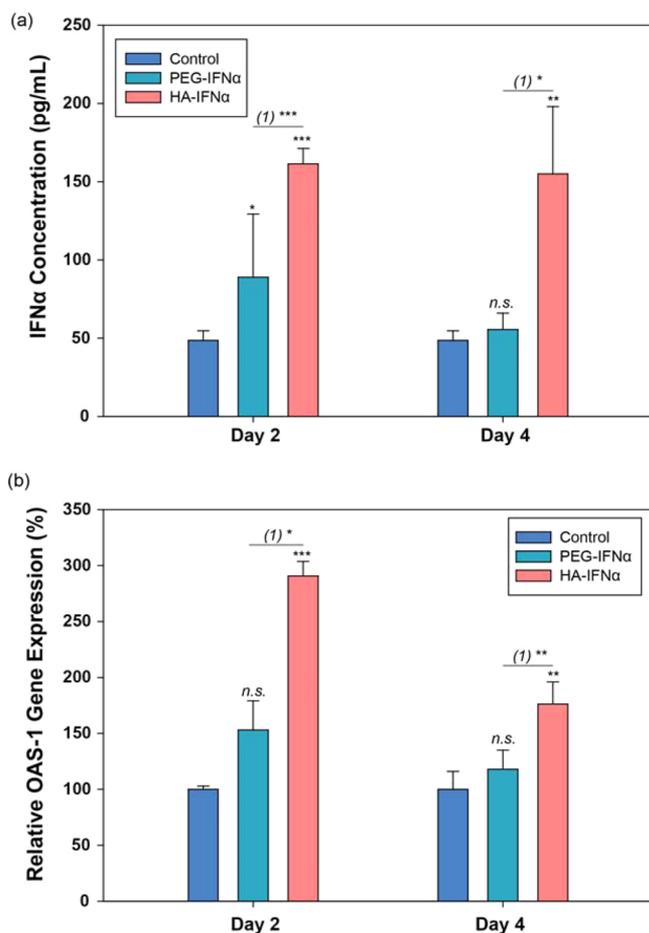
**Long-Term Biodistribution of the HA-IFN $\alpha$ -ZW800-1 Conjugate.** Because the HA-IFN $\alpha$ -ZW800-1 conjugate showed the highest rate of uptake to the liver 24 h postinjection, we further investigated the long-term clearance of the conjugate in the body (Figure 7). SD rats were injected



**Figure 7.** (a) Intraoperative fluorescence images and (b) quantitative analysis for long-term biodistribution and clearance of HA-IFN $\alpha$ -ZW800-1 conjugates for up to 10 days after intravenous injection. Abbreviations: He, heart; Lu, lung; Li, liver; Sp, spleen; Pa, pancreas; Ki, kidney; Du, duodenum; In, intestine.

intravenously with 50 nmol of the HA-IFN $\alpha$ -ZW800-1 conjugate and sacrificed every 24 h up to 10 days. The fluorescence intensity in the liver was the highest at day 1 postinjection and gradually decreased over the course of 10 days. The results were well matched with our previous data as reported elsewhere.<sup>11</sup> All the remaining tissues and organs except liver, kidney, and spleen showed very minimal uptake, reflecting the possibility of the HA-IFN $\alpha$ -ZW800-1 conjugate for target-specific treatment of liver diseases without potential side effects by nonspecific uptake. Despite wide applications of IFN $\alpha$  and PEG-IFN $\alpha$  for the treatment of HCV infection, the repeated injection was known to cause significant side effects, including renal dysfunction and capillary leak syndrome.<sup>33,34</sup>

**In Vivo Antiviral Effect of HA-IFN $\alpha$  Conjugates.** As a feasibility study for clinical applications, HA-IFN $\alpha$  conjugates were subcutaneously injected into SD rats for the analysis of IFN $\alpha$  content by an ELISA and OAS1 mRNA levels by real-time PCR in the liver tissues 2 and 4 days postinjection (Figure 8). After injection of the HA-IFN $\alpha$  conjugate, the amount of IFN $\alpha$  was 3.3- and 1.8-fold higher in the liver than those of the control and PEG-IFN $\alpha$  in 2 days, respectively, reflecting the target-specific delivery of HA-IFN $\alpha$  conjugates to the liver (Figure 8a). In contrast, PEG-IFN $\alpha$  was not detected so much in the liver compared to HA-IFN $\alpha$  conjugates. As is well-known,



**Figure 8.** (a) Pharmacokinetic analysis of PEG-IFN $\alpha$  and HA-IFN $\alpha$  conjugates by an ELISA in the liver after subcutaneous injection. PBS was used as a negative control. (b) Relative level of OAS1 mRNA in the liver by RT-PCR after subcutaneous injection of the control of PBS, PEG-IFN $\alpha$ , and HA-IFN $\alpha$  conjugate. Statistical analysis was conducted for the control vs PEG-IFN $\alpha$  and HA-IFN $\alpha$  conjugates (\* $P < 0.05$ ; \*\* $P < 0.01$ ; \*\*\* $P < 0.001$ ). (1) represents PEG-IFN $\alpha$  vs HA-IFN $\alpha$  conjugate.

PEGylation is intended to bypass the liver for long-term circulation of IFN $\alpha$  in the body. The results indirectly indicate that HA-IFN $\alpha$  conjugates can be more effective than PEG-IFN $\alpha$  for the treatment of HCV infection.

After that, the antiviral activity of HA-IFN $\alpha$  conjugates was investigated by measuring the level of OAS1 mRNA in the liver using RT-PCR. The antiviral activity of IFN $\alpha$  is highly related to the expression of OAS1, which is the essential protein for innate immune responses to viral infection.<sup>30,35,36</sup> Figure 8b shows the relative expression levels of the OAS1 gene by RT-PCR after subcutaneous injection of the control, PEG-IFN $\alpha$ , and HA-IFN $\alpha$  conjugate. In accordance with the biodistribution data, the OAS1 mRNA level increased more significantly after subcutaneous injection of the HA-IFN $\alpha$  conjugate than the control and PEG-IFN $\alpha$ . The results were well matched with our previous data after intravenous injection of the HA-IFN $\alpha$  conjugate.<sup>30</sup> The elevated level of OAS1 mRNA was maintained for >4 days (Figure 8b). With the data taken together, we could confirm the feasibility of the HA-IFN $\alpha$  conjugate for the treatment of HCV infection and possibly hepatocellular carcinoma.<sup>25,26</sup>

## CONCLUSION

We have successfully investigated the intrinsic biodistribution and clearance of the HA-IFN $\alpha$  conjugate for the treatment of HCV infection using a zwitterionic and nonsticky NIR fluorophore of ZW800-1. The short-term and long-term delivery and accumulation of the HA-IFN $\alpha$  conjugate in the liver were significant because of the synergistic effect of HA and IFN $\alpha$  receptors in the liver. The long-term *in vivo* and *ex vivo* bioimaging was also helpful for understanding the fate of bioconjugates, i.e., biodistribution and clearance in each tissue. Furthermore, we could confirm the antiviral activity of HA-IFN $\alpha$  conjugates from the elevated level of OAS1 mRNA in the liver by the analysis of RT-PCR. All these results lay the foundation for investigating the pharmacokinetics and efficacy of the HA-IFN $\alpha$  conjugate as a new therapeutic drug for the treatment of HCV infection and possibly hepatocellular carcinoma.

## ASSOCIATED CONTENT

### Supporting Information

The Supporting Information is available free of charge on the ACS Publications website at DOI: 10.1021/acs.biomac.5b00933.

Additional observations and results (PDF)

Real-time biodistribution and excretion of ZW800-1 over a 4 h time lapse (AVI)

Real-time biodistribution and excretion of HA-IFN- ZW800-1 over a 4 h time lapse (AVI)

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### Notes

The authors declare no competing financial interest.

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## REFERENCES

- (1) Tan, S.-L.; Pause, A.; Shi, Y.; Sonenberg, N. Hepatitis C therapeutics: current status and emerging strategies. *Nat. Rev. Drug Discovery* **2002**, *1*, 867–881.
- (2) Gravitz, L. Introduction: A smoldering public-health crisis. *Nature* **2011**, *474*, S2–S4.
- (3) Perz, J. F.; Armstrong, G. L.; Farrington, L. A.; Hutin, Y. J. F.; Bell, B. P. The contributions of hepatitis B virus and hepatitis C virus infections to cirrhosis and primary liver cancer worldwide. *J. Hepatol.* **2006**, *45*, 529–538.
- (4) Fellay, J.; Thompson, A. J.; Ge, D.; Gumbs, C. E.; Urban, T. J.; Shianna, K. V.; Little, L. D.; Qiu, P.; Bertelsen, A. H.; Watson, M.; Warner, A.; Muir, A. J.; Brass, C.; Albrecht, J.; Sulkowski, M.; McHutchison, J. G.; Goldstein, D. B. ITPA gene variants protect against anaemia in patients treated for chronic hepatitis C. *Nature* **2010**, *464*, 405–408.

- (5) Thomas, D. L.; Thio, C. L.; Martin, M. P.; Qi, Y.; Ge, D.; O'Huigin, C.; Kidd, J.; Kidd, K.; Khakoo, S. I.; Alexander, G.; Goedert, J. J.; Kirk, G. D.; Donfield, S. M.; Rosen, H. R.; Tobler, L. H.; Busch, M. P.; McHutchison, J. G.; Goldstein, D. B.; Carrington, M. Genetic variation in IL28B and spontaneous clearance of hepatitis C virus. *Nature* **2009**, *461*, 798–801.
- (6) Schlutter, J. Therapeutics: New drugs hit the target. *Nature* **2011**, *474*, S5–S7.
- (7) Wang, Y.-S.; Youngster, S.; Grace, M.; Bausch, J.; Bordens, R.; Wyss, D. F. Structural and biological characterization of pegylated recombinant interferon alpha-2b and its therapeutic implications. *Adv. Drug Delivery Rev.* **2002**, *54*, 547–570.
- (8) Bailon, P.; Palleroni, A.; Schaffer, C. A.; Spence, C. L.; Fung, W.-J.; Porter, J. E.; Ehrlich, G. K.; Pan, W.; Xu, Z.-X.; Modi, M. W.; Farid, A.; Berthold, W.; Graves, M. Rational Design of a Potent, Long-Lasting Form of Interferon: A 40 kDa Branched Polyethylene Glycol-Conjugated Interferon  $\alpha$ -2a for the Treatment of Hepatitis C. *Bioconjugate Chem.* **2001**, *12*, 195–202.
- (9) Foser, S.; Schacher, A.; Weyer, K. A.; Brugger, D.; Dietel, E.; Marti, S.; Schreitmuller, T. Isolation, structural characterization, and antiviral activity of positional isomers of monopegylated interferon alpha-2a (PEGASYS). *Protein Expression Purif.* **2003**, *30*, 78–87.
- (10) Yang, J.-A.; Park, K.; Jung, H.; Kim, H.; Hong, S. W.; Yoon, S. K.; Hahn, S. K. Target specific hyaluronic acid–interferon alpha conjugate for the treatment of hepatitis C virus infection. *Biomaterials* **2011**, *32*, 8722–8729.
- (11) Oh, E. J.; Park, K.; Kim, K. S.; Kim, J.; Yang, J.-A.; Kong, J.-H.; Lee, M. Y.; Hoffman, A. S.; Hahn, S. K. Target specific and long-acting delivery of protein, peptide, and nucleotide therapeutics using hyaluronic acid derivatives. *J. Controlled Release* **2010**, *141*, 2–12.
- (12) Stern, R. Hyaluronan catabolism: a new metabolic pathway. *Eur. J. Cell Biol.* **2004**, *83*, 317–325.
- (13) Goh, E. J.; Kim, K. S.; Kim, Y. R.; Jung, H. S.; Beack, S.; Kong, W. H.; Scarcelli, G.; Yun, S. H.; Hahn, S. K. Bioimaging of Hyaluronic Acid Derivatives Using Nanosized Carbon Dots. *Biomacromolecules* **2012**, *13*, 2554–2561.
- (14) Kim, J.; Kim, K. S.; Jiang, G.; Kang, H.; Kim, S.; Kim, B.-S.; Park, M. H.; Hahn, S. K. In vivo real-time bioimaging of hyaluronic acid derivatives using quantum dots. *Biopolymers* **2008**, *89*, 1144–1153.
- (15) Kim, K. S.; Hur, W.; Park, S.-J.; Hong, S. W.; Choi, J. E.; Goh, E. J.; Yoon, S. K.; Hahn, S. K. Bioimaging for Targeted Delivery of Hyaluronic Acid Derivatives to the Livers in Cirrhotic Mice Using Quantum Dots. *ACS Nano* **2010**, *4*, 3005–3014.
- (16) Kim, K. S.; Kim, S.; Beack, S.; Yang, J.-A.; Yun, S. H.; Hahn, S. K. In vivo real-time confocal microscopy for target-specific delivery of hyaluronic acid-quantum dot conjugates. *Nanomedicine* **2012**, *8*, 1070–1073.
- (17) Choi, H. S.; Ipe, B. I.; Misra, P.; Lee, J. H.; Bawendi, M. G.; Frangioni, J. V. Tissue- and Organ-Selective Biodistribution of NIR Fluorescent Quantum Dots. *Nano Lett.* **2009**, *9*, 2354–2359.
- (18) Soo Choi, H.; Liu, W.; Misra, P.; Tanaka, E.; Zimmer, J. P.; Iyengar, B.; Bawendi, M. G.; Frangioni, J. V. Renal clearance of quantum dots. *Nat. Biotechnol.* **2007**, *25*, 1165–1170.
- (19) Choi, H. S.; Gibbs, S. L.; Lee, J. H.; Kim, S. H.; Ashitate, Y.; Liu, F.; Hyun, H.; Park, G.; Xie, Y.; Bae, S.; Henary, M.; Frangioni, J. V. Targeted zwitterionic near-infrared fluorophores for improved optical imaging. *Nat. Biotechnol.* **2013**, *31*, 148–153.
- (20) Choi, H. S.; Nasr, K.; Alyabyev, S.; Feith, D.; Lee, J. H.; Kim, S. H.; Ashitate, Y.; Hyun, H.; Patonay, G.; Strekowski, L.; Henary, M.; Frangioni, J. V. Synthesis and In Vivo Fate of Zwitterionic Near-Infrared Fluorophores. *Angew. Chem., Int. Ed.* **2011**, *50*, 6258–6263.
- (21) Tanaka, E.; Choi, H. S.; Humblet, V.; Ohnishi, S.; Laurence, R. G.; Frangioni, J. V. Real-time intraoperative assessment of the extrahepatic bile ducts in rats and pigs using invisible near-infrared fluorescent light. *Surgery* **2008**, *144*, 39–48.
- (22) Ballou, B.; Fisher, G. W.; Deng, J. S.; Hakala, T. R.; Srivastava, M.; Farkas, D. L. Cyanine fluorochrome-labeled antibodies in vivo: assessment of tumor imaging using Cy3, Cy5, Cy5.5, and Cy7. *Cancer Detect. Prev.* **1998**, *22*, 251–257.
- (23) Warren, A.; Le Couteur, D. G.; Fraser, R.; Bowen, D. G.; McCaughan, G. W.; Bertolino, P. T lymphocytes interact with hepatocytes through fenestrations in murine liver sinusoidal endothelial cells. *Hepatology* **2006**, *44*, 1182–1190.
- (24) Gaumet, M.; Vargas, A.; Gurny, R.; Delie, F. Nanoparticles for drug delivery: The need for precision in reporting particle size parameters. *Eur. J. Pharm. Biopharm.* **2008**, *69*, 1–9.
- (25) Damdinsuren, B.; Nagano, H.; Wada, H.; Noda, T.; Natsag, J.; Marubashi, S.; Miyamoto, A.; Takeda, Y.; Umeshita, K.; Doki, Y.; Dono, K.; Monden, M. Interferon alpha receptors are important for antiproliferative effect of interferon- $\alpha$  against human hepatocellular carcinoma cells. *Hepatol. Res.* **2007**, *37*, 77–83.
- (26) Melén, K.; Keskinen, P.; Lehtonen, A.; Julkunen, I. Interferon-induced gene expression and signaling in human hepatoma cell lines. *J. Hepatol.* **2000**, *33*, 764–772.
- (27) Gisslinger, H.; Kurzrock, R.; Gisslinger, B.; Jiang, S.; Li, S.; Virgolini, I.; Woloszczuk, W.; Andreeff, M.; Talpaz, M. Autocrine cell suicide in a Burkitt lymphoma cell line (Daudi) induced by interferon  $\alpha$ : involvement of tumor necrosis factor as ligand for the CD95 receptor. *Blood* **2001**, *97*, 2791–2797.
- (28) Bell, S. J.; Fam, C. M.; Chlipala, E. A.; Carlson, S. J.; Lee, J. I.; Rosendahl, M. S.; Doherty, D. H.; Cox, G. N. Enhanced Circulating Half-Life and Antitumor Activity of a Site-Specific Pegylated Interferon- $\alpha$  Protein Therapeutic. *Bioconjugate Chem.* **2008**, *19*, 299–305.
- (29) Glue, P.; Fang, J. W. S.; Rouzier-Panis, R.; Raffanel, C.; Sabo, R.; Gupta, S. K.; Salfi, M.; Jacobs, S. Pegylated interferon-[ $\alpha$ ]2b: Pharmacokinetics, pharmacodynamics, safety, and preliminary efficacy data[ast]. *Clin. Pharmacol. Ther.* **2000**, *68*, 556–567.
- (30) Yang, J. A.; Park, K.; Jung, H.; Kim, H.; Hong, S. W.; Yoon, S. K.; Hahn, S. K. Target specific hyaluronic acid-interferon alpha conjugate for the treatment of hepatitis C virus infection. *Biomaterials* **2011**, *32*, 8722–9.
- (31) Wüthrich, R. P. The proinflammatory role of hyaluronan–CD44 interactions in renal injury. *Nephrol. Dial. Transpl.* **1999**, *14*, 2554–2556.
- (32) Oliver, G. Lymphatic vasculature development. *Nat. Rev. Immunol.* **2004**, *4*, 35–45.
- (33) Dusheiko, G. Side effects of  $\alpha$  interferon in chronic hepatitis C. *Hepatology* **1997**, *26*, 1125–121S.
- (34) Lechner, J.; Krall, M.; Netzer, A.; Radmayr, C.; Ryan, M. P.; Pfaller, W. Effects of interferon [ $\alpha$ ]-2b on barrier function and junctional complexes of renal proximal tubular LLC-PK1 cells. *Kidney Int.* **1999**, *55*, 2178–2191.
- (35) Yuan, L.; Wang, J.; Shen, W.-C. Lipidization of human interferon-alpha: A new approach toward improving the delivery of protein drugs. *J. Controlled Release* **2008**, *129*, 11–17.
- (36) Shrivastava, S.; Raychoudhuri, A.; Steele, R.; Ray, R.; Ray, R. B. Knockdown of autophagy enhances the innate immune response in hepatitis C virus–infected hepatocytes. *Hepatology* **2011**, *53*, 406–414.